

Successful Adaptation of a Group EEG Generative Model to Individuals Depends on Participant Typicality

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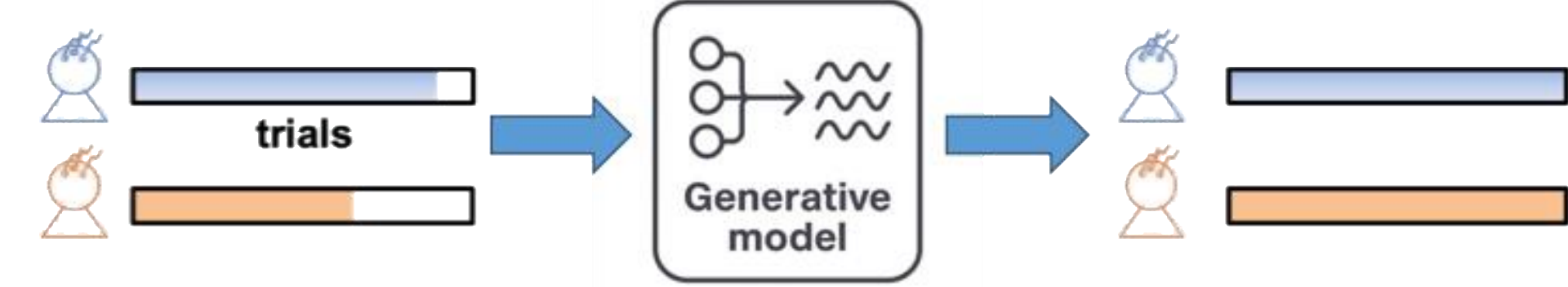
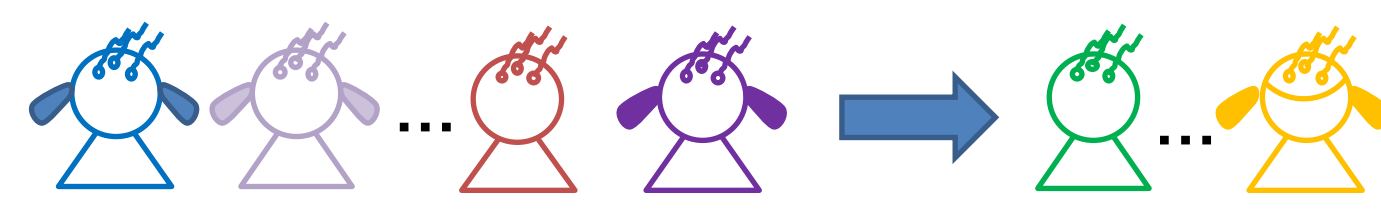
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Introduction

Machine learning can be used to identify patterns in EEG data. However, sometimes **there is insufficient data to do this**.

- **Case1:** not enough patients: **generate artificial EEG data at the individual level**
- **Case 2:** not enough trials per participant: **generate artificial EEG data at the trial level**



Problem: how to generate participant-specific EEG trials for different conditions with individual physiological plausibility?

Methods

1 Dataset and preprocessing

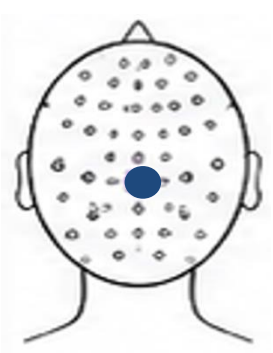
Public EEG dataset [1]

visual search task

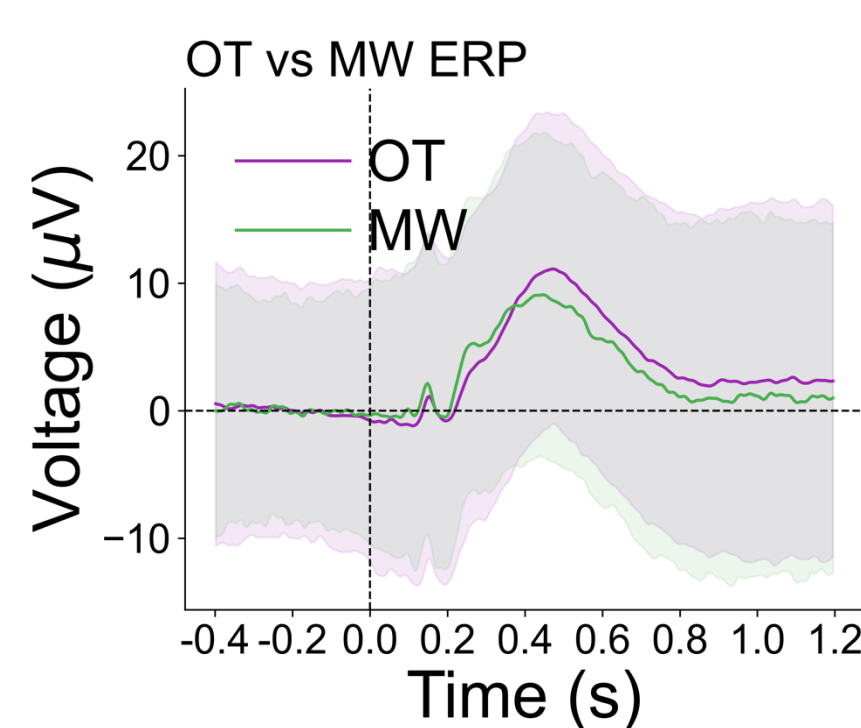
thought-probe labels: OT vs. MW

OT 4753 trials
(25 eligible participants)

MW 1789 trials
(12 eligible participants)

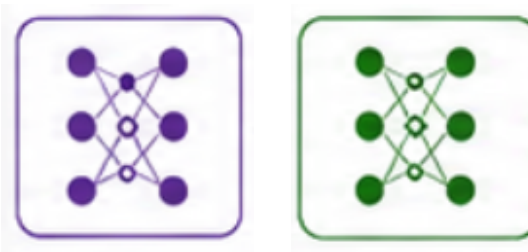
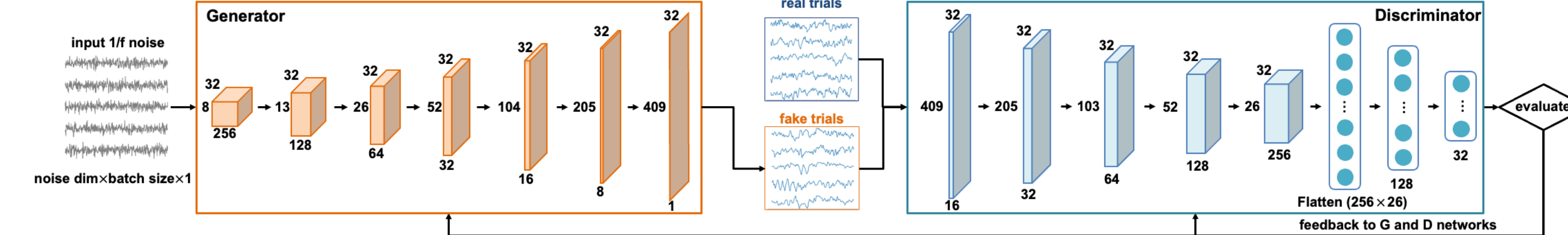


- Single channel (near Pz)
- 256 Hz sampling rate
- 1600 ms trials
- Re-reference (average)
- 0.5-40 Hz band-pass filter
- ICA artifact removal



2 Group-pretrained models

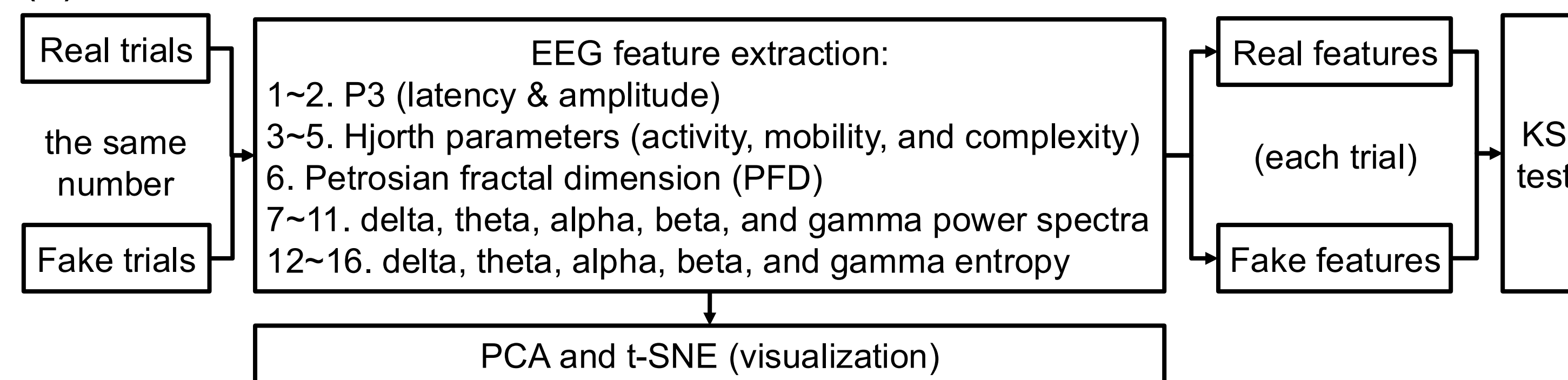
ERP-WGAN-GP [2]



Full fine-tuning (all parameters updated)

4 Fake trial evaluation

- (1) waveform inspection; (2) ERP and PSD plot evaluation;
(3) extracted EEG feature evaluation;



- (4) quantitative similarity metrics (Real vs. Fake)

• $PCA-overlap_{RF}$, $PCA-BC_{RF}$, $PCA-JS_{RF}$, SWD , $MMD-RBF$, WD

Fine-tuning quality was based on $PCA-overlap_{RF}$:

Good: ≥ 0.60 ; Borderline: $0.50-0.60$; Poor: < 0.50 .

5 Participant-level predictor analysis

Predictors computed from **real data** only

Predictors (per participant)

- 16 feature deviations
- 2D PCA_{PG} centroid distance
- 16D centroid distance
- ERP deviation
- PSD deviation
- Mahalanobis distance
- Local density



Spearman correlation

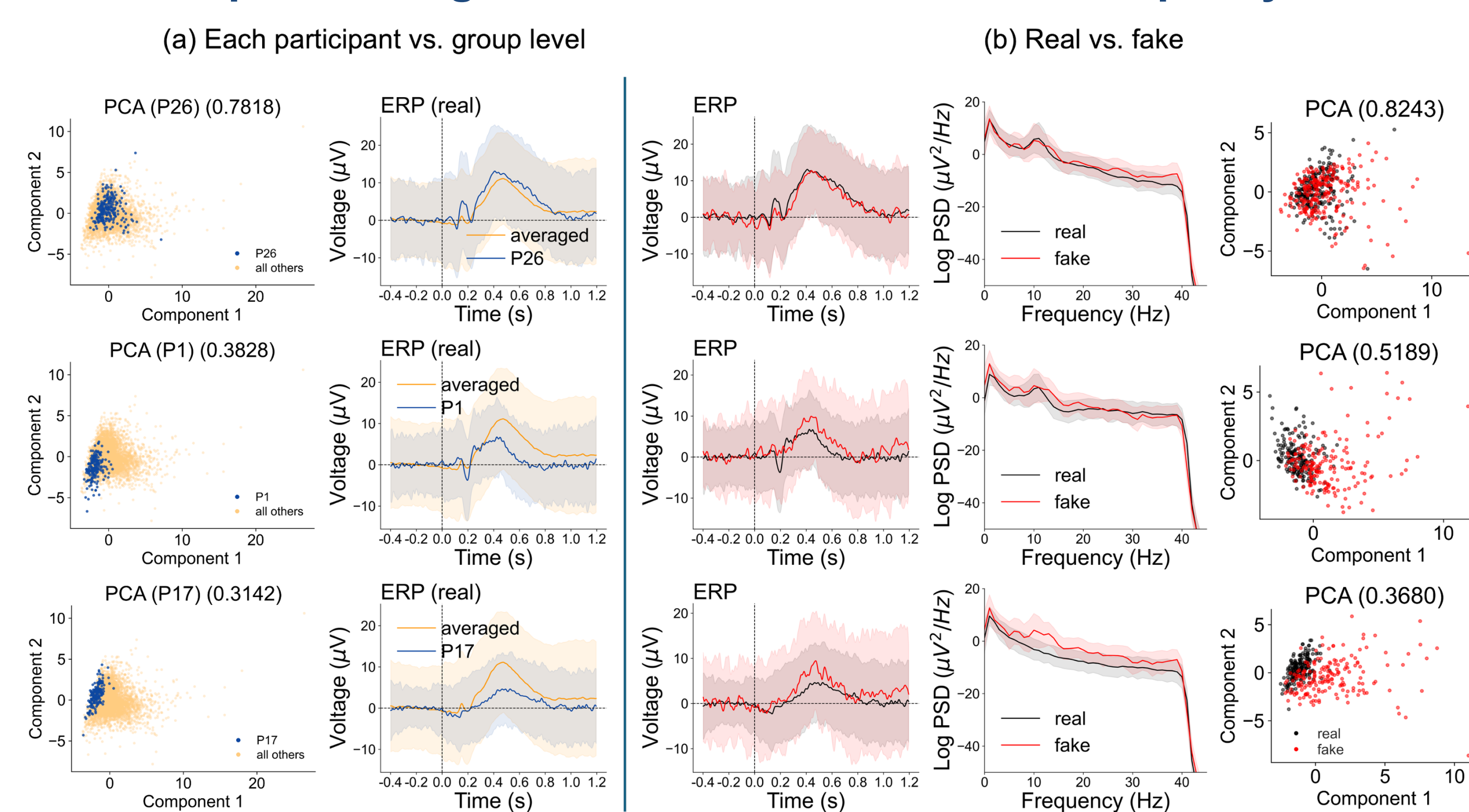
Outcome: $PCA-overlap_{RF}$

Metric Abbreviation

BC: Bhattacharyya coefficient
JS: Jensen-Shannon divergence
MMD-RBF: maximum mean discrepancy with radial-basis-function kernel
PCA: principal component analysis
PG: participant-group; **RF:** real-fake
SWD: sliced Wasserstein distance
WD: time-point-wise Wasserstein distance

Results

OT examples linking PG real-data deviation and RF quality



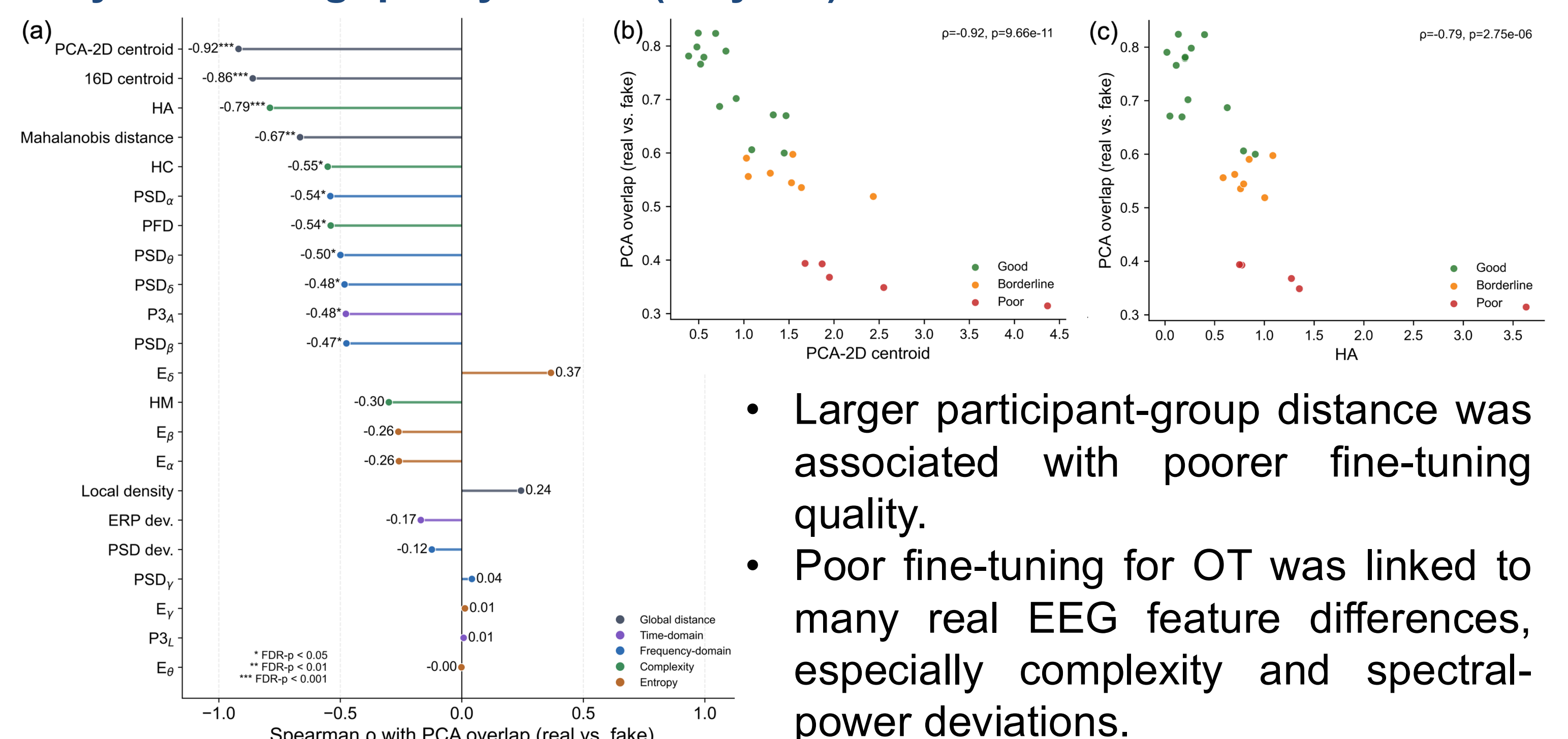
- Participants differ in how well the group-level model transfers.
- Participant 26 (P26), closer to the **group-level** feature distribution center, shows a good real-fake ERP and PS match.
- Participant 17 (P17), at the edge of the **group-level** feature distribution, shows a poor real-fake ERP and PS match.

Fake-trial quality metrics across participants for OT and MW fine-tuning

Task condition	n	$PCA-overlap_{RF} \uparrow$	$PCA-BC_{RF} \uparrow$	$PCA-JS_{RF} \downarrow$	$SWD \downarrow$	$MMD-RBF \downarrow$	$WD \downarrow$
OT	25	0.6090 ± 0.1575	0.8394 ± 0.1083	0.1402 ± 0.0911	3.0133 ± 0.9194	0.0225 ± 0.0126	2.5862 ± 0.9273
MW	12	$0.6887 \pm 0.0534^*$	$0.9102 \pm 0.0232^*$	$0.0831 \pm 0.0214^*$	2.4985 ± 0.6446	$0.0141 \pm 0.0050^*$	2.0966 ± 0.7617

Values are reported as mean $\pm$ standard deviation. arrows: direction of better quality, n: number of eligible participants. Welch's two-sample t-test was used for OT-MW fine-tuning comparison. Benjamini-Hochberg false discovery rate-corrected significance level: * $p < 0.05$.

Why fine-tuning quality varies (only OT)



- Larger participant-group distance was associated with poorer fine-tuning quality.
- Poor fine-tuning for OT was linked to many real EEG feature differences, especially complexity and spectral-power deviations.

Conclusion

- Group-pretrained EEG generative models (ERP-WGAN-GP) can be fine-tuned to individual participants.
- Fine-tuning is not always successful: MW showed stable real-fake agreement, whereas OT showed larger participant-level variability.
- For the OT condition, larger participant-to-group real EEG deviation is associated with poorer fine-tuning quality.
- Participant-to-group deviation may help identify when individualized EEG generation is feasible.



LinkedIn

Abbreviation:

EEG: electroencephalogram; **ERP:** event-related potential
G: Generator; **D:** Discriminator; **WD:** Wasserstein distance
ICA: independent component analysis;
KS test: Kolmogorov-Smirnov test
MW: mind-wandering; **OT:** on-task; **PSD:** power spectral density
t-SNE: t-distributed stochastic neighbor embedding
WGAN-GP: Wasserstein generative adversarial networks with gradient penalty

References:

- [1] Jin, Christina Yi, Jelmer P. Borst, and Marieke K. Van Vugt. "Predicting task-general mind-wandering with EEG." Cognitive, Affective, & Behavioral Neuroscience 19 (2019): 1059-1073.
- [2] Li, X., van Vugt, M. K., & Maurits, N. M. "Evaluating the impact of input noise and ERP-based penalties on the physiological plausibility of EEG generation using WGAN-GP." Computers in biology and medicine 199 (2026): 111296.